

7: Two compartment modeling

1. What is compartmental modeling ?
2. How can tracer kinetics be mathematically described ?
3. How do 2-deoxyglucose methods trace glucose metabolism ?

After this course you

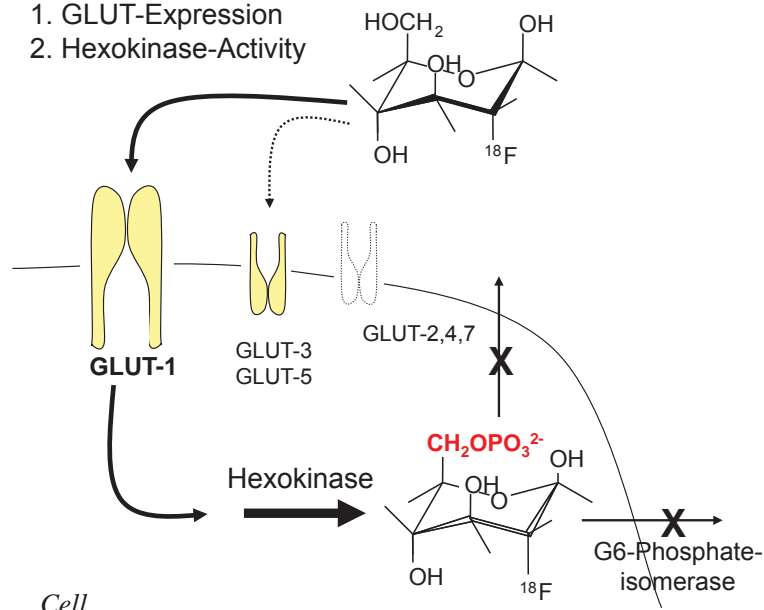
1. Understand how mass conservation can be used to model tracer kinetics and estimate metabolic rates
2. Understand the mathematical principle underlying metabolic modeling of imaging data
3. Can apply the principle of modeling tracer uptake to simple kinetic situations
4. Understand the basics of modeling deoxyglucose uptake into tissue to extract metabolic rates

How is intracellular glucose metabolism measured ?

$[^{18}\text{F}]\text{FDG}$ (2- $[^{18}\text{F}]$ Fluoro-2-Deoxy-Glucose)

FDG uptake depends on:

1. GLUT-Expression
2. Hexokinase-Activity



7-1. What is a compartment model ?

tracers

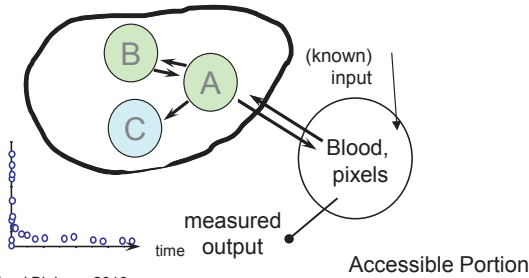
Definition: Compartment

Concept: Physiological system - decomposed into N interacting subsystems

Subsystem = chemical species in a physical place (**compartment**)

NB. Tracer is considered to be distributed uniformly in compartment

Inaccessible portion



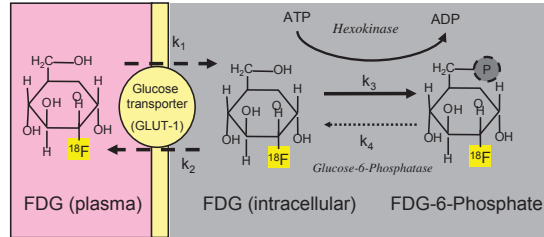
Key elements of compartmental modeling

1. Predict inaccessible features of system
2. Measurement in the accessible portion
3. Estimation of specific *parameters of interest*.

Steady-state assumption:

1. metabolic rate of process is not changing with time
2. concentrations are constant during the evaluation period.

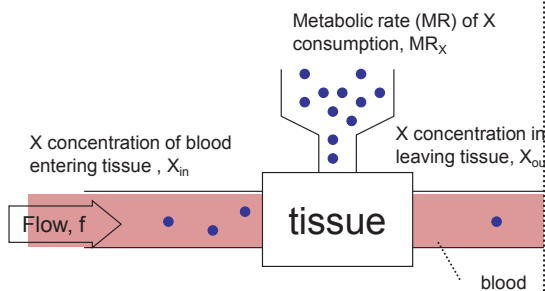
processes can be described with pseudo-first-order rate constants.



How does conservation of mass allow rate determination ?

Fick's principle

Fick Principle (steady state conditions)



$$MR_x = f \times \{ [X]_{in} - [X]_{out} \}$$

X = O₂, glucose, ammonia, water

Brain physiology: O₂ consumption increases less than Flow

Q: What is the consequence?

$$[O_2]_{entering} - [O_2]_{leaving} = \frac{\text{rate of } O_2 \text{ consumption}}{\text{Flow}}$$

Definition Tracer

- radio-activity emitting, labelled molecule
- structurally related to the natural substance (*tracee*) or involved in the dynamic process

See earlier examples, but also O₂ (left)

introduced in a trace amount (=orders of magnitude below tracee); process being measured is not perturbed by it.

few tracer molecules contain radioactive isotope; others contain "cold" isotope

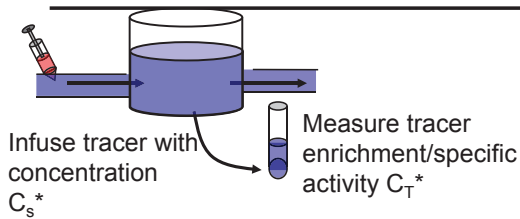
Specific activity (SA) = "hot" / "cold" tracer molecules

SA is always measured; [MBq/μmol or mCi/μmol]

→ convert measured radioactivity concentrations in tissue and blood to mass (correct for physical decay)

7-2. What are first-order tracer kinetics ?

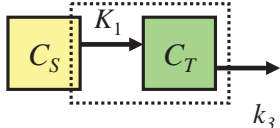
One-tissue compartment model



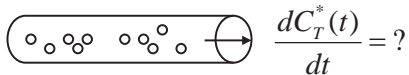
The rate of labeled molecules entering C_T
 $dC_T^*/dt =$ Metabolic flux $V \times$ probability of precursor C_S labeled

$$\frac{dC_T^*(t)}{dt} = V \frac{C_S^*}{C_S} = K_1 C_S^*(t)$$

Unidirectional chemical reaction $S \rightarrow T$:



How many labeled (red) molecules/per min ? (Assume the rate is $V=10/\text{min}$)



First-order process $S \rightarrow T$

Reaction velocity $V [\mu\text{mol/g/min}] : k \equiv V/C$

$$V = \frac{dC_T(t)}{dt} = K_1 C_S(t) - k_3 C_T(t)$$

K_1, k_3 - (pseudo) first-order rate constants;

\Rightarrow independent of concentration and time;
 unit: $[\text{sec}^{-1} \text{ or } \text{min}^{-1}]$

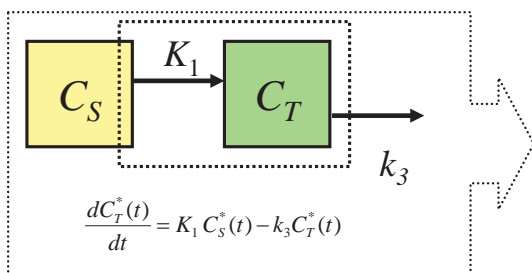
Need to add efflux from C_T :

k_3 : Metabolic efflux $V \times$ probability of molecule C_T being labeled

$$\frac{dC_T^*(t)}{dt} = K_1 C_S^*(t) - k_3 C_T^*(t)$$

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What describes the one-tissue compartment model ?



Linear first-order ordinary differential equations (ODEs):

\rightarrow Laplace transformation

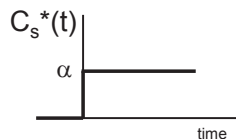
$$C_T^*(t) = K_1 C_S^*(t) \otimes e^{-k_3 t}$$

$$a(t) \otimes b(t) = \int_0^t a(\tau) b(t-\tau) d\tau$$

Example:

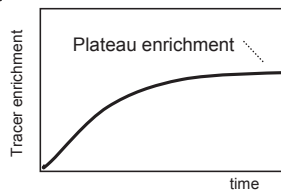
C_S^* increased from 0 to α at $t=0$

$$\frac{dC_T^*(t)}{dt} = k_1 \alpha - k_3 C_T^*(t)$$



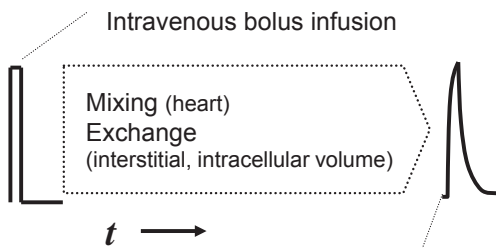
$$C_T^*(t) = \frac{k_1 \alpha}{k_3} (1 - e^{-k_3 t})$$

$C_T^*(0)=0$



7-7

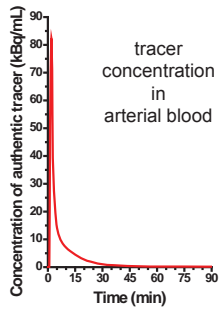
What is the input function ?



Tracer: injected intravenously (as a bolus, i.e. Short time period)

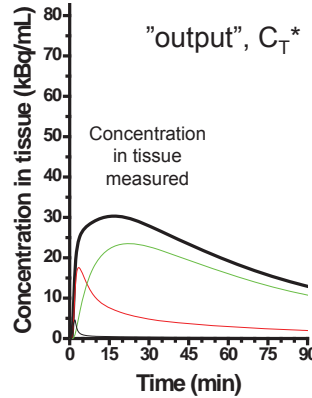
1. well mixed with blood (heart)
2. distributed to capillary bed \rightarrow exchange with tissue
3. Tracer concentration in tissue increases by extraction of tracer from plasma
4. Concentration in tissue is reduced by backward transfer

Measured arterial plasma (arterial input function) C_S^*



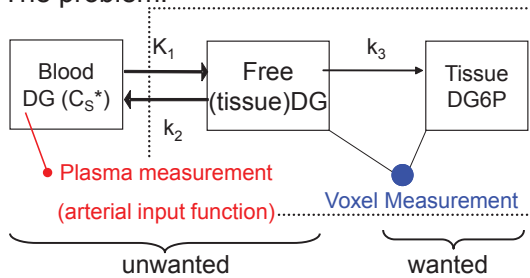
Uptake into tissue, e.g.
Perfusion
Endothelial permeability
Vascular volume fraction
Transport across cell membranes

Specific binding to receptors
Non-specific binding
Enzyme activity



7-3. How does Deoxyglucose (DG) measure glucose metabolism ? (autoradiography, FDG PET)

The problem:

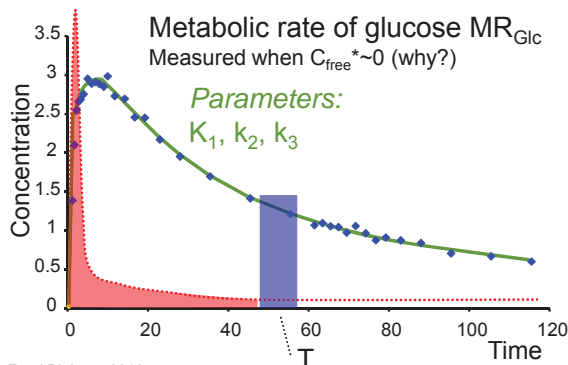


$$\frac{dC_{free}^*(t)}{dt} = K_1 C_S^*(t) - (k_2 + k_3) C_{free}^*(t)$$

$$\frac{dC_T^*(t)}{dt} = k_3 C_{free}^*(t) \quad C_T^*(T) = k_3 \int_0^T C_{free}^*(t) dt$$

Rapid glucose transport : $C_S^*(t) \cong C_{free}^*(t)$

$$MR_{Glc} \propto k_3 \quad k_3 = \frac{C_T^*(T)}{\int_0^T C_S^*(t) dt}$$



$$MR_{Glc} = \frac{C_S}{LC} \frac{C_T^*(T)}{\int_0^T C_S^*(t) dt}$$

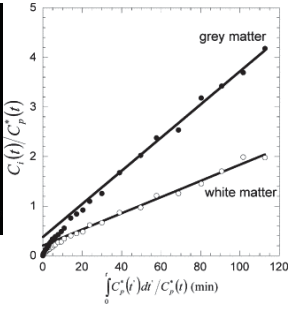
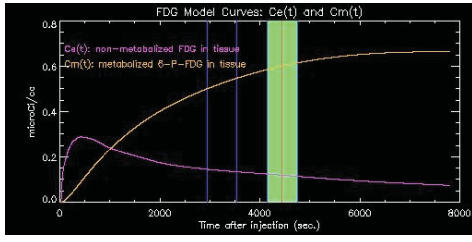
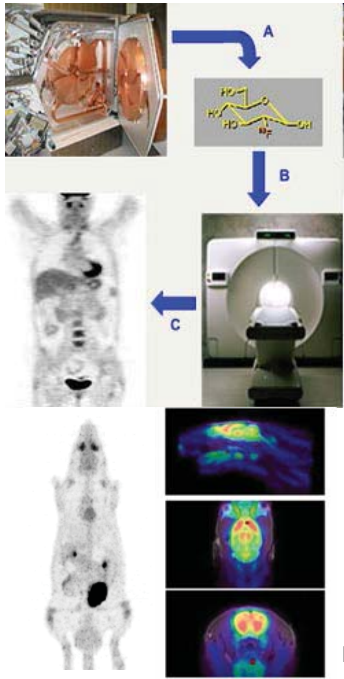
Lumped constant (LC): differences between glucose and DG

(affinities for transporters and hexokinase)

C_S : blood glucose concentration

$$\text{Unit of } MR_{glc}: [MR_{glc}] = \frac{\mu\text{mol Glc}}{\text{mL tissue} \times \text{min}}$$

Ex. Typical FDG PET scan



45 min uptake phase (minimal tissue FDG) then scan FDG-6P

Raw PET values		<p>plane # 17, microCi/cc</p>	Model results for C(t)	
avg:	0.274104		T (secs):	3090
num:	59447		C(t):	0.274104
min:	0.00000		Ce(T):	0.000422
max:	0.537945		Cm(T):	0.353923
thresh:	0.177522		ICMRight:	5.64327
thresh%:	0.330000	<input checked="" type="checkbox"/> Link DK-Cor to PET		

Rodent FDG PET